Precision and practical usefulness of intraoral scanners in implant dentistry: A systematic literature review

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Abstract

Background: This systematic review aimed to evaluate the efficiency and accuracy of digital impression techniques for implant-supported restorations, and to assess their economic feasibility.

Material and Methods: Two independent electronic database searches were conducted in the Pubmed/MedLine, Cochrane Library, and Lilacs databases complimented by a manual search, selecting relevant clinical and in vitro studies published between 1st January 2009 and 28st February 2019. All type of studies (*in vivo* and *in vitro*) were included in this systematic review.

Results: Twenty-seven studies (8 in vivo and 19 in vitro studies) fulfilled the inclusion criteria. No meta-analysis was performed due to a large heterogeneity of the study protocols. The passive fit of superstructures on dental implants presented similar results between digital and conventional impression techniques. The studies considered that several factors influence the accuracy of implant impression taking: distance and angulation between implants, depth of placement, type of scanner, scanning strategy, characteristics of scanbody, and operator experience. Regarding the economic viability of intraoral scanning systems, only one study reported any benefit in comparison with conventional techniques.

Conclusions: Digital impressions of dental implants can be considered a viable alternative in cases of one or two contiguous dental implants. However, more studies are needed to evaluate the accuracy of digital techniques in full-arch implant-supported restorations.

Key words: Intraoral scanner, dental implant, prosthesis, misfit, systematic review.

Introduction

It is many years since the long-term success of dental implants was confirmed by Branemark et al. and Albrektsson et al. (1,2) Since then, numerous studies have described new surgical and prosthodontic techniques that aim to improve the clinical outcomes of implant-based treatments (3,4). In cases of implant-supported restorations, treatment success depends on the superstructure's passive fit, as failure to achieve adequate passive fit can produce biological and mechanical complications (5). Fit depends on the accuracy of implant impression taking, which may be realised using long-established conventional techniques or more recently introduced digital techniques. The fabrication of an implant-supported prosthesis in a conventional workflow must start with the aid of an implant transfer post. Conventional impression taking can be classified as direct (pick-up) or indirect (transfer).

With the introduction of digital technologies in dentistry, intraoral scanners can now be used for digital impression taking. According to the manufacturers, the use of intraoral scanners are a key element in the digital workflow, providing greater comfort for the patient, decreased turnaround time, and even a better cost-benefit ratio when compared to conventional techniques (6). But to date, no systematic literature review has been conducted to confirm the advantages of digital impression taking. In this context, this systematic literature review aimed to: (a) to determine if it is possible to achieve an adequate level of accuracy and efficiency using intraoral digital impression systems and to compare them with various conventional techniques for implant-supported restorations and (b) to assess the economic feasibility of digital techniques.

Material and Methods

This systematic review was conducted following PRIS-MA guidelines (7) and was registered in the Prospero database (trial no. CRD42015029504). The systematic review focused question was based on the PICO format (Population, Intervention, Comparison, Outcome) as follows:

Population: healthy adult human patients.

Intervention: conventional impression techniques.

Comparison: digital impression taking with intra-oral scanners.

Outcome: accuracy of impression and efficiency for fixed implant-supported restorations.

-Study Selection Criteria

In order to identify relevant articles, the following inclusion criteria were applied: Clinical studies without language restriction that evaluated the accuracy of digital impressions taken with intraoral scanners or compared digital impression taking with conventional impression taking in treatment protocols leading to fixed implant-supported restorations. As the initial search generated only a few articles, and so insufficient scientific evidence, the search was extended to include *in vitro* studies. Finally, due to the heterogeneity of different articles it was not possible implement a meta-analysis.

-Search Strategy

An electronic search was conducted in the following databases: PubMed, Cochrane Library, Lilacs. Key search terms were applied, combined using MesH terms, to locate relevant articles published between 1st January 2009 and 28st February 2019. A additional manual search was conducted in the following journals: Clinical Implant Dentistry and Related Research, International Journal of Oral & Maxillofacial Implants, Journal of Oral Implantology, Clinical Oral Implants Research, Journal of Dental Research, Clinical Oral Implants Research, European Journal of Oral Implantology, Implant Dentistry, International Journal of Oral and Maxillofacial Surgery, Journal of Oral Implantology, Journal of Dentistry, Clinical Oral Investigations, and Journal of Oral Rehabilitation. All the corresponding authors of the studies identified were contacted in order to ascertain if additional articles or unpublished data were available.

-Data Collection and Quality Assessment

The search was carried out by two independent reviewers. Any disagreement between the reviewers (IGG and JC-BB) regarding data collection or quality assessment was resolved by consensus. Inter-reviewer reliability was assessed obtained a Kappa coefficient of 0.88 (CI 95%), values above 0.8 being considered a good level of agreement (8). To assess the quality of in vivo articles, the Critical Appraisal Skills Program (CASP) proposed by the Public Health Resource Unit (2006) was used, and only studies with an overall score of at least 50% were included in the review. Due to the small number of in vivo studies available, a duplicate search was performed to obtain in vitro studies. Although in vitro research cannot reproduce the dynamic environment of the stomatognathic system or human variability, pre-clinical experiments can provide important information about the properties and characteristics of a new material or technique. It is therefore necessary to conduct in vitro research of the highest possible standard. Efforts have been made in recent years to improve the quality of reporting in scientific literature (9,10). Although the CASP consort checklist was not originally designed for analyzing in vitro trials, in 2012 a modified consort checklist was published of items selected to assess reporting in vitro studies of dental materials.18 The authors of the present review adapted this checklist for the purpose of comparing the accuracy of different dental implant impression-taking techniques. Only studies with an overall score of at least 50% were included in the review.

Results

-Included Studies

An electronic search of the PubMed/MedLine, Cochrane Library and Lilacs databases located 1358 articles, which were reduced to 40 following title, abstract and full text analysis (PubMed/MedLine n=29; Lilacs n=7; Cochrane Library n=4). The articles from the different databases were compared to identify any duplicates, and a further 11 articles were eliminated on the basis of duplication (n=11) (Fig. 1). The ten remaining *in vivo* articles were categorized as follows: systematic reviews (n=5), randomized clinical trials (RCT) (n=1), prospective cohort studies (n=1), case-control studies (n=2), and case reports (n=1).

The corresponding authors of the selected studies were contacted via email of whom four returned additional data. However, no additional data was included for analysis as all proved to be either replicate information or failed to meet the inclusion criteria. Due to the small number of *in vivo* studies available, the search was extended to include in vitro studies, using the same method, selecting 20 additional in vitro studies. These authors were also contacted via email, generating further data in three cases (n=3), but these were not included in the review for the same reasons as before. A modified CONSORT checklist of items for reporting in vitro studies was used to evaluate the risk of bias in the *in vitro* studies included (Fig. 2). When applying this modified CONSORT checklist to in vitro articles, points 5-9 could not be applied as they were designed to evaluate sample standardization. In the in vitro studies, the master model was the same in each study group, and so always standard. Of the articles evaluated, only one19 did not exceed the minimum score for inclusion in the review



Fig. 1: Numbers of articles in databases.

Section	Checklist item
Abstract	A Structured summary of trial design, methods, results, and conclusions
Introduction	B Scientific background
	C Objectives and/or hypotheses
Methods	D The intervention for each group, with sufficient detail
	E How and when the primary and secondary measures are evaluated
	F Statistical methods used to compare groups for primary and secondary outcomes
Results	G For each primary and secondary outcome, results for each group, and the estimated size of the effect and its precision
Discussion	H Trial limitations, addressing sources of potential bias, imprecision, and, if relevant, multiplicity of analyses
Other information	I Sources of funding and other support
	J Where the full trial protocol can be accessed

Fig. 2: Modified consort Checklist in vitro studies.

(5/10), obtaining a score of 0/10 and so was eliminated (Table 1). Finally, the review included eight *in vivo* and 19 *in vitro* studies. The reasons for exclusion of various articles are specified in (Table 2).

-Outcomes

Implant impressions can be obtained using open or closed tray, with or without splinting, using different impression materials (CI) or scanbody + an intraoral scanner system (DI). In order to carry out a complete analysis of the included articles, the outcomes were divided according to the technique(s) investigated: DI (17 studies), or CI vs. DI (12 studies) (Tables 3,4).

1. DI

Seventeen studies used DI to take impression of dental implants: five systematic reviews, one case report, and eleven *in vitro* studies.

In Vivo

This case report describes DI in a patient with a fully edentulous jaw rehabilitated with six dental implants; three clinical tests were carried out to evaluate the accuracy of the superstructure: saliva intrusion, the Sheffield test, and the screw resistance test, although the authors did not specify the fit values obtained (11).

In Vitro

Eleven *in vitro* studies were located that investigated the accuracy of IOS, divided into three subgroups: partially edentulous (PE), completely edentulous (CE), and partially and completely edentulous models (CE-PE). *In Vitro* - PE

Three in vitro studies used DI-PE models (12-14).

In 2012, Van der Meer *et al.* (12) carried out a study using a PE model with the aim of evaluating the accuracy of three different IOS. The authors concluded that the Lava COS was more accurate than the other IOS. Flugge *et al.* (13) employed two models bearing dental implants to compare the precision of three IOS with a laboratory scanner, obtaining a decrease in precision of the IOS when the distance between scan bodies increased, whereas with the dental lab scanner this was not dependent. Koch *et al.* (14). compared volumetric

Author	Abstract	Introduction		Methods					
	1	2. A.	2. B.	3	4	5	6	7	8
Chia et al. (30)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Menini et al. (34)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Marghalini et al. (31)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Imburgia et al. (22)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Amin <i>et al.</i> (33)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Chew et al. (29)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Vandeweghe <i>et al.</i> (20)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Gimenez-Gonzalez et al. (19)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Mangano et al. (21)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Flugge et al. (13)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Koch et al. (14)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Papaspyridakos <i>et al.</i> (32)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Gimenez et al. (18)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Gimenez et al. (17)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Gimenez et al. (16)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Lin et al. (28)	YES	YES	YES	YES	NO	NO	NO	NO	NO
Lee et al. (27)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Rauscher et al. (40)	NO	NO	NO	NO	NO	NO	NO	NO	NO
Gimenez et al. (15)	YES	YES	YES	YES	YES	NO	NO	NO	NO
Van der Meer <i>et al.</i> (12)	YES	YES	YES	NO	NO	NO	NO	NO	NO

Table 1: Modified checklist used to assess quality and risk of bias of in vitro studies.

Table 2: Studies excluded and reasons for exclusion.

STUDIES	REASON FOR EXCLUSION
Eliasson and Ortorp, 2012; Ramsey and Ritter, 2012; Al-	Use of healing abutments.
Abdullah, Zandparsa et al.; 2013; Howell, McGlumphy	
et al., 2013; Nayyar, Yilmaz et al., 2013; Derhalli, 2013;	
Abdel-Azim, Zandinejad et al., 2014; Ajioka, Kihara et al.,	
2016.	
Ortorp, Jemt et al., 2005; Bergin, Rubenstein et al., 2013.	Intraoral Scanner no longer available commercially
Lee and Gallucci, 2013; Lee, Macarthur et al., 2013;	Evaluated efficiency or difficulty of scanning operation or
Joda, Lenherr et al., 2017.	scanning learning curve.
Wismeijer, Mans et al. 2014; Joda and Bragger, 2015;	Evaluated patient preference for conventional or digital
Schepke, Meijer et al. 2015.	technique
Stimmelmayr, Erdelt et al., 2012; Stimmelmayr, Guth et al.,	Use of extraoral scanner, not intraoral scanner
2013; Jokstad and Shokati, 2015.	

deviations between single tessellation language (STL) datasets of a master model, and milled model, and IOS from a previous single implant model. The authors concluded that direct digitization using the IOS presented less systematic error than physical model fabrication by milling from IOS.

In Vitro - CE

Six *in vitro* studies used digital techniques to scan CE models (15-20).

In the studies carried out by Giménez *et al.*, (15-19) precision was assessed in an edentulous maxillary model with different implant angulations. The same authors (15)

Table 3: In vivo stud	lies.							
AUTHOR Flugge et al. (39) Muhlemann et al. (38) Rutkunas et al. (36)	STUDY DESIGN Systematic Review Systematic Review Systematic Review	MAX/MB	POSITION OF DENTA	LIMPLANT	EDENTULISM	N° IMPLANTS/PATHENT - -	IMPLANT BRAND -	CONNECTION
Alikhasi et al. (37) Gherlone et al. (26) Gherlone et al. (25) Joda et al. (6) Andriessen et al. (24) Moreno et al. (11)	Systematic Review Randomized Clinical Pilot Study Prospective Cohorts Pilot Study Case Report	- LTMAX/MB MAX/MB TMAX/MB MB MB	#35, #32, #45 or #15 #35, #32, #45 or #15 Premolar and Molar #33, #43 No data	, #12, #22, #25 , #12, #22, #25	Compl. Compl. Partial. Compl. Compl.	- 120 impl. / 25 patients 16 impl. / 14 patients 1 implant / 20 patient 2 implant / 25 patient 6 implant / 1 patient	No data Winsix (BioSAFin) Straumann TL RN/WN Straumann TL RN/WN Exfeel External, Megagen Implant	- External Internal Internal External
AUTHOR Flugge et al. (39) - Muhlemann at al. (38)	ANGULATION IMPL. PLA	ACEMENT DE	PTH CONVENTIONAL or	DIGITAL IMPRES	SION SPT or NSP1	r SPT MATERIAL SPT METH -	OD METHOD IMPRESSION MATER	AL IMPRESION
wunnemann et al. (30) Rurkunas et al. (37) Alikhais et al. (37) Gherlone et al. (26) Inder et al. (25) Joda et al. (6) Handressen et al. (24) Moreno et al. (11)	Parallel / 30- 35° No. Parallel / 30- 35° No. Parallel / 30- 35° No. Vo data No.	data data data data data	- CT immedite loading + D CT immedite loading + D CT + DI D1 D1	I Imediate Loading I final restauration				ita
AUTHOR Flugge et al. (39) Muhlemann et al. (38) Rutkunas et al. (36)	SCANNER SYSTEM / SO. -	FTWARE NU	MBER OF IMPRESSION	IMPRESSION AC -	CURACY			
Alikhasi et al. (37) Gherlone et al. (26) Joda et al. (25) Joda et al. (6) Andriessen et al. (24) Moreno et al. (11)	TRIOS// No data TRIOS// No data Tero // No data Tero // Software 3.5 0. LAVA C.O.S // No data	- 20 N N O	data data data	- No data No data No data Mean Distance Err No data	or 226.0µm and Distan	tee error ranging (21-638µm); Mear	Angulation Error 2.582° and Angulation er	or ranging (0.123-9.563°,
AUTHOR SCANNER Flugge et al. (39) - Muhlemann et al. (38)	SYSTEM / SOFTWARE NUMBER OF	7 IMPRESSION IM.	PRESSION ACCURACY			ACCURACY M	THOD	e-Mail CASP - 7 - 9
Altkhase et al. (35) Altkhase et al. (37) Gherbore et al. (28) TRIOS/ No Gherbore et al. (28) LEAVC.CDS Joba et al. (6) Andriessen et al. (11) LAVAC.OS Moreno et al. (11) LAVAC.OS	data No data - No fata - No data No data	No NN NN NN NN NN NN NN NN NN NN NN NN N	data data un Distance Error 2260µm and Distance errort data	ranging (21-638µm); Mean Ar	gulation Error 2.582° and Angula	X Ray (muoranti, X Ray (muoranti, X Ray (muoranti, X Ray (muoranti, X Ray (muoranti) X Ray (muoranti) X Ray (muoranti) Rocking of the fra	ratiographs) with prostheses and a bur-implant connection and S ratiographs) with prostheses and a bur-implant connection. County 12, 32 Systems nework not be deceted. Sheffield test, X-Ray.	8 veficield test. yees 7 yes 7 8 8
AUTHOR Flugge et al. (39)	ACCURACY METHOD				e-Mail CAS - 7	SP		
Muhlemann et al. (38) Rutkunas et al. (36) Alikhasi et al. (37) Gherlone et al. (26) Gherlone et al. (25)	- - X-Ray (panoramic radiogra X-Ray (panoramic radiogra	ahs) with prosth	sses and a bar-implant connecti eses and a bar-implant connect	ion and Sheffield tes ion.	9 yes 8 yes 7 yes 7 7			
Andriessen et al. (24) Moreno et al. (11)	Software Geomagic Qualify Rocking of the framework n	12, 3D System of be detected, 5	s Sheffield test, X-Ray.		0 F 8			
Conventional Impre tially edentulous (Pa	ssions (CI), Digital Im art.), Completely edent	pressions (D) ulous (Comp	 Intraoral Scanning (I. I.), Bone Level (BL), Tis 	OS), Maxilla (N ssue Level (TL)	1AX), Mandible (, Splinted (SPT)	MB), Coordinate measuren , Not Splinted (NSPT), Ope	nent machine (CMM), PEEK Scan n Tray (OT), Closed Tray (CT), Sc	Bodies (PEEK), Par- an Body (SB), Vinyl

polysiloxane (VPS), Polyether (PE), Plaster Impression (P), Acrylic Resin (AR), Light polymerizing acrylic resin (LAR), Auto-polymerizing acrylic tray resin (AAR), Resin bars (RB), SD (Standard Desviation).

	viiro	/ studies											
AUTHOR Menini et al. (34)		STUDY In vitro	MAX/MB MAX	POSITION OF 1 #16, #13, #23, #2	DENTAL 6, in 1 cas	IMPLANT t		EDENTULIS Compl.	M Nº IMPI 4	IMPLANT BRAND Biomet 3i		CONNECTIO External	N ANGULATION IMPL. Parallel
Chia et al. (30)		In vitro	MB	#44, #46 in 3 cas	L			Part.	2	Straumann BL		Internal	0, 10, 20 degrees buccolingual
Marghalini et al. (31 Imburgia et al. (22))	In vitro In vitro	MB MAX	#34, #36, in 2 cas Model 1 (PEM):	its #23. #24			Part. Part. & Compl	2	Nobel Biocare& Straum BT Safe Int, BTK-Bioter	ann TL c Implants	Internal	0, 30 degrees No data
Amin et al. (33)		In vitro	мв	Model 2 (FEM): #31, #32, #35, #4	#16, #14, 2, #45, in	#11,#21, #24, #2 1 cast	26	Compl.	5	Straumann BL	e impiants	Internal	#31, #32, #42: 0° // #35: 10° distally // #45: 15° distally
Chew et al. (29)		In vitro	MB	#44, #45, in 1 cas	at			Part.	2	Straumann BL and TL		Internal	Parallel
Vandeweghe et al. (2 Gimenez-Gonzalez e	20) et al. (19	In vitro) In vitro	MB MAX	#46, #44, #42,#32 #17, #15, #12, #2	2, #34, #30 2, #25, #2	5, in 1 cast 7, in 1 cast		Compl. Compl.	6 6	IBT (Southern Implants) Biomet 3i		External Internal	Parallel #17, #12, #22, #27: 0° // #15: 30° distally // #25: 30° mesially
Mangano et al. (21)		In vitro	MAX	Model 1 (PEM): Model 2 (FEM):	#21, #24, #16, #14,	#26 #11,#21, #24, #2	26	Part. & Compl	. 3,6	BTK implants		No data	No data
Flugge et al. (13)		In vitro	MB	Model 1: #36, #3 Model 2: #36, #3 #25_in 1_cost	5 5,#33,#45	i,#47		Part.	2,5	Straumann BL		Internal	No data
Papaspyridakos et al	l. (32)	In vitro	MB	#31, #32, #35, #4	2, #45, in	1 cast		Compl.	5	Straumann BL		Internal	#31, #32, #42: 0° // #35: 10° distally // #45: 15° distally
Gimenez et al. (18) Gimenez et al. (17)		In vitro In vitro	MAX MAX	#17, #15, #12, #2 #17, #15, #12, #2	2,#25,#2 2.#25.#2	7, in 1 cast 7, in 1 cast		Compl. Compl.	6	Biomet 3i Biomet 3i		Internal Internal	#17, #12, #22, #27: 0° // #15: 30° distally // #25: 30° mesially #17, #12, #22, #27: 0° // #15: 30° distally // #25: 30° mesially
Gimenez et al. (16)		In vitro	MAX	#17, #15, #12, #2	2,#25,#2	7, in 1 cast		Compl.	6	Biomet 3i		Internal	#17, #12, #22, #27: 0° // #15: 30° distally // #25: 30° mesially
Lin et al. (28) Lee et al. (27)		In vitro In vitro	MB MAX	#35, #37, in 4 cas #25, in 1 cast	its			Part. Part.	2	Straumann TL Straumann BL		Internal	Model 1: 0°, model 2: 15°, model 3: 30°, model 4: 45° No data
Gimenez et al. (15) Van das Maas et al. (12)		In vitro	MAX	#17, #15, #12, #2 # 36 #41 #46 ii		12, #25, #27, in 1 cast		Compl.	6	Biomet 3i		Internal	#17, #12, #22, #27: 0° // #15: 30° distally // #25: 30° mesially No data
van der Meer et al. ((12)	in vitro	MD	# 50, #41, #40, II	I cast.			Part.	3	No data		NO data	ino data
AUTHOR Menini et al. (34)	P N	LACEMENT I lo data	DEPTH		CI or DI CI + DI	SPT or NSPT SPT and NSPT	SPT AR	MATERIAL S	PT METHOD	METHOD IMPRESSION OT-SPT, OT-NSPT, CT, IOS	MATERI/ PE ; P / SE	AL IMPRESION	SCANNER SYSTEM / SOFTWARE True Definition // no data
Chia et al. (30)	В	8L			CI + DI	SPT	AAF	R -		OT / IOS	VPS / SB		Trios COLOR // v3.1.4
Marghalini et al. (31) Imburgia et al. (22)	N N	lo data lo data			CI + DI DI	SPT -	LAR -	R -		OT-SPT / IOS IOS	PE / SB PEEK Sca	n Bodies	CEREC Omnicam, True Definition// no data CS 3600, Trios 3, CEREC Omnicam, True Definition// no data
Amin et al. (33) Chew et al. (29)	N N	io data io data			CI + DI CI + DI	SPT SPT	LAR AAF	R R R -	В	OT / IOS OT / IOS	PE / SB PE / SB		CEREC Omnicam/ 4.4.1; True Definition/ 4.1 Trios COLOR/v3.1.4; iTero/ v HD 2.9; True Definition/ no data
Vandeweghe et al. (20) Gimenez-Gonzalez et al Mangano et al. (21)	N 1.(19) # n	lo data 17, #15, #25, #2 o data	7: 0mm // #12:	4mm // #22: 2mm	DI DI DI	-	-	-		IOS IOS IOS	PEEK SB PEEK SB PEEK SB		True Definition, LAVA C.O.S., CEREC Omnicam, Trios//no data True Definition//no data Trios, CS 3500, Zfx Intrascan, Planmeca PlanScan, Richardson TX//no data
Flugge et al. (13)	Ν	io data			DI	-	-	-		IOS	SB		True Definition, Itero, Trios//no data
Koch et al. (14) Papaspyridakos et al. (3	N N	io data			DI CI + DI	- SPT and NSPT	- I A R	- 2 P	в	IOS OT-SPT OT-NSPT IOS	SB PF / SB		iTero//no data Trios//no data
Gimenez et al. (18)	(2) I #	17, #15, #25, #2	7: 0mm // #12:	4mm // #22: 2mm	DI	-	-		5	IOS	PEEK SB		LAVA Chairside Oral Scanner// V 0.3.0.2
Gimenez et al. (17) Gimenez et al. (16)	#	17, #15, #25, #2	7: 0mm // #12: 7: 0mm // #12:	4mm // #22: 2mm 4mm // #22: 2mm	DI	-	-			IOS	PEEK SB PEEK SB		CEREC AC Bluecam/CEREC 4.0
Lin et al. (28) Lee et al. (27)	1 N	mm coronal io data			CI + DI CI + DI	No data NSPT	2	-		OT OT/IOS	VPS / SB VPS / SB		iTero//Straumann Cares 8.0 iTero//no data
Gimenez et al. (15) Von der Meer et al. (12)	#	17, #15, #25, #2	7: 0mm // #12:	4mm // #22: 2mm	DI	-	-	-		IOS	PEEK SB		iTero//v 4.5.0.151 iTero/ 2.5.0: 1.4VA COS/ 2.1: CEREC Rhacom/ 2.85
AUTHOR	NUMBER	OF IMPRESSION	IMPRESSION /	CCURACY	51					100	T LEAC OD		new 555, Elin Cost El, Chile Bilenin 555
Menini et al. (34)	5 each oper	rator	Distance error M Angle error Mean	ean±SD (mm): OTNSPT1-I a±SD (*): OTNSPT1-PE (0.	PE(-0.021±0.03 252±0.196); O	0); OTSPT1-PE (-0.032 FSPT1-PE (0.129±0.091	2±0.033 1) ; CT1	 ; CT1-PE (0.031±0.0 1-PE (0.361±0.217); OT 	9); OTNSPT2-PE (NSPT2-PE (0.536±	0.010±0.053); OTSPT2-PE (-0.060±0.037 0.378); OTSPT2-PE (0.503±0.854); CT2-	7); CT2-PE(-0.0 PE(0.322±0.18	14±0.026); OT-P(0.059±0 i); OT-P(0.110±0.090); D	.034); DI (-0.012±0.026) I (0.257±0.242)
Chia et al. (30)	5 CI and 51	DI	Mean 3D desviat Absolute angular	ion (mm)±SD:DS0°(0.031± distorsion (X), (Y) (°)±SD:	0.0142); DS10 DS0°(0.041±0	(0.045±0.0034); DS20° .0318), (0.103±0.0649);	(0.042± DS10)	±0.0099);CI0\(0.0018±0) (0.546±0.2705), (0.111)	1.0084); C110°(0.033 t0.0639); DS20°(0.1	±0.0158); CI20°(0.036±0.0065) 94±0.2739), (0.075±0.0615);CI0°(0.073±	0.0618), (0.195	0.1317); CI10°(0.275±0.	2957), (0.106±0.0773); CI20*(0.545±0.0615), (0.166±0.1343)
Imburgia et al. (22)	5 for each r	n model model	PEM(µm): CS36 FEM (µm):CS36	00 (45.8 ± 1.6), Trios 38 (50) 00 (45.8 ± 1.6), Trios 38 (50) 008 (60.6 ± 11.7), Omnica	i), Omnicam (2) (2 ± 2.5), Omr n⊗ (66.4 ± 3.9)	icam® (58.8 ± 1.6) and . Trios3® (67.2 ± 6.9).	and Stri TrueDe TrueDe	raumann [C1 (22 ± 5), Of refinition® (61.4 ± 3.0) efinition® (106.4 ± 23.1	nncam (26±15), 11	ue D. (17 ±5)]			
Amin et al. (33) Chew et al. (29)	10 for each 5 for each r	i model model	Mean value (µm) Global linear dist	: CI (167.93)(SD 50.37); O orsion (µm): BLCI(35±6); I	mnicam (46.41 BLTrios(64 ± 1)(SD 7.34); True Definit 0); BLiTero(62 ± 18);Bl	tion (19 LTrueD	9.32)(SD 2.77) 0(63 ± 17); TLCI (49 ±	0); TLTrios (58 ± 1	1); TLiTero(66 ± 34);TLTrueD(64 ± 16)			
Vandewerhe et al. (20)	10 for each	model	Absolute angular Absolute angular Mean trueness: L	distorsion (Y) (°): BLCI(0) distorsion (X) (°): BLCI(0) ava COS[0,112 mm (SD 0.)	058±0.031); BI 09±0.082); BL 025)1, 3M True	Trios(0.105±0.058); BI Trios(0.206±0.044); BLi Def.10.035 mm (SD 0.0	LiTero(0 iTero(0. (12)1.38	0.191±0.124);BLTrueD (154±0.113);BLTrueD(0 Shape 10.028 mm (SD 0	0.315±0.138); TLC 0.226±0.143); TLCI .007)]. Cerec Omnis	I(0.186±0.161); TLTrios(0.089±0.039); TL 0.196±0.147); TLTrios(0.066±0.033); TL am [0.061 mm (SD 0.023)]// mean precis	iTero(0.203±0. iTero(0.160±0.1 ion: Lava COSI	094')(TLTrueD(0.206±0. 21)(TLTrueD(0.195±0.14 0.066 mm (SD 0.025)), 3	115') 0) M TrueDef./0.030 mm (SD 0.011)1. 3Shane(0.033 mm (SD 0.012)). Cerec Omnicam(0.059 mm (SD (
Gimenez-Gonzalez et al. (19) Mangano et al. (21)	20 for each 5 for each r	i model model	Distance Mean D PEM: CS3500 (tr FEM/CS 25008)	esviation (µm): 1°quadrant ueness 47.8 µm, precision	7.6± (SD 17.6 10.8 µm); Trios); 2° quadrant(-10.3± (S ® (trueness 71.2 μm, pr	SD 39.2 recision	t)). // Angulation Mean 51.0 μm), Zfx Intrasca	Desviation (*): 1°qui 1® (trueness 117.0 p	drant(-0.021± (SD 0.17)); 2° quadrant(-0) im, precision 126.2 µm), and Planscan® (028± (SD 0.16) trueness 233.4 µ	m, precision 219.8 µm)	
Flugge et al. (13)	10 for each	model	Mean Distance(n Mean Angle and	(trueness 6.3.2 µm, precisio im) and SD (µm): iTero [(D SD (*): iTero [(ACA1: 8.06	n 55.2 µm), 1n IP1: 6.669 (28 (0.18)): (ACA	osso (trueness 71.6 µm,); (DIP2: 11.209 (26)); 2: 2.35 (0.22)); (ACA3:	(DIP3: 8.19 (0	6.783 (28)); (DIP4: 17. (.24)); (ACA4: 8.85 (0.2	canio (trueness 103. 596 (26)); (DIP5: 10 (2)); (ACA5: 15.23)	0 µm, precision 112.4 µm), and Planscano (990 (30)); (DIP6: 40.608 (28)); (DIP7: 5 0.29)); (ACA6: 17.47 (0.21)); (ACA7: 23	6 (trueness 255) 0.479 (64))] and 1.09 (0.20))] and	True Definition [(DIP1: True Definition [(ACA1)). 5.647 (4)); (DIP2: 11.224 (5)); (DIP3: 6.778 (7)); (DIP4: 17.610 (9)); (DIP5: 10.999 (5)); (DIP6: 40.5 8.20 (0.044); (ACA2: 2.46 (0.10)); (ACA3: 8.12 (0.10)); (ACA4: 8.75 (0.10)); (ACA5: 15.35 (0.09));
Koch et al. (14) Papaspyridakos et al. (32)	30 for each 10 for each	i model i model	Volumetric desvia Mean 3D Desvia	ations (mm): Master vs Mas tion (µm): Group I (OTSPT	ter (0.000±0.0 BL) [7.42 (5.2	01); Master vs IOS (-0.0 8–10.88)]; Group II (C	001±0.0 OPNSPI	(21); IOS vs milled (-0. T-BL) [17.65 (13.19–76)	008±0.098); Maste (49)]; Group III (DI	vs milled (-0.010±0.100) BL) [19.38 (11.54-26.21)]; Group IV (O	TSPT-Abutment	level)[13.05 (10.46-23.6	7)]; Group V (OTNSPT-Abutment level) [8.23 (4.01–12.13)]
Gimenez et al. (18) Gimenez et al. (17) Gimenez et al. (16)	5 each oper 5 each oper	rator erator	Mean Desviation Mean Desviation	DI vs Master model(µm): e DI vs Master model(µm) Z	FX Intrascan v	3.8 ± (SD 25.9)); inexpe s 3D Progress: experien	ced (-11	d (13.3 ± (SD 51.2)); an 79 ± (SD 601) vs 249±	gulated (-20.2 ± (SI (SD 702)); inexperie	(21.9)); paralell (-37.9 ± (SD 26.2)); deep nced (-101 ± (SD 705) vs 224± (SD 930)); angulated (-12 47 + 105 50); 22	± (SD 18.7)); gingival mi 5 ± (SD 596) vs 257± (S	rgmail level (-28.5 ± (SD 29.8)) D 776)); paralell (-150 ± (SD 693) vs 224± (SD 854)); deep implant (-150 ± (SD 397) vs 87 ± (SD 40. 2 0 02); deep implant (-150 ± (SD 693) vs 224± (SD 854)); deep implant (-150 ± (SD 397) vs 87 ± (SD 40.
Lin et al. (28) Lee et al. (27)	10 for each 30	i model	Linear difference Volumetric desvia	s DI vs CI (µm): 0° (221±3) ation Horizontal: CI (0.034;	5); 15° (260±35 ±0.009 mm) vs); 30° (159±36); 45° (75 DI (0.011±0.013 mm)//	5±36) // Volume	Angular differences DI etric desviation Vertical	vs CI (*): 0° (0.986: CI (-0.088 ± 0.044	(1.84.3 ± 99.9); 0mm impaint deput (1.89.5 (0.218); 15° (1.551±0.218); 30° (0.004±0; mm) DII (0.093±0.061 mm)	218); 45° (0.438	±0.218)	± 30.52); 4000 miljuni uepu (-107.25 ± 08.05); 1 quantum (-17 ± 20.5); 2 quantum (-110 ± 105)
Gimenez et al. (15) Van der Meer et al. (12)	5 each ope 10	rator	Distance desviati Mean distance en Mean absolute an	on and SD (µm): (#27-#25: ror (µm): [Lava COS [(#4.6 gulation errors (°): [Lava C	-14.3 (SD25.6) - #4.1): 14.6(S OS: [(#4.6 - #4	i; (#27-#22:-16.2 (SD34 D 12.7)(95% CI: 6.7-2; .1): 0.2049 (SD 0.0440)	4.6));(#2 2.4)]; [()(95% C	27-#12:-27.9 (SD61.6)) (#4.6 - #3.6): 23.5(SD 1 CI: 0.1776-0.2322)]; [(#	(#27-#15:-23.21 (S) 4.2)(95% CI: 14.7- 4.6 - #3.6): 0.4722	0148));(#27-#17:-32 (SD216.1)) // Distan (2.3)]]; [CEREC bluecam [(#4.6 - #4.1): 7 SD 0.1436) (95% CI: 0.3831– 0.5612)]; [ce desviation an 19.6(SD 77.1)(9: CEREC bluecar	d SD (µm) implant depth % CI: 31.8–127.4)] ; [(# n:[(#4.6 - #4.1): 0.6303 ()	$\begin{array}{l} (0mm23.1 (8D149.485)); (2mm16.2 (8D34569)); (4mm27.9 (8D61.643)) \\ (5.6 + 33.6); 81.6 (8D 52.5) (95\% CI: 49.1-114.2))]; (Tero 1 (#4.6 + 34.1); 70.5 (8D 56.3) (95\% CI: 35.5-10.04396) (95\% CI: 0.2884 - 0.6367)); [10.04399) (95\% CI: 0.2884 - 0.6367), [10.04399) (95\% CI: 0.2884 - 0.6367), [10.04397) (95\% CI: 0.2884 - 0.6367), [10.04370) (95\% CI: 0.2884 - 0.6367), [10.04397) (95\% CI: 0.2884 - 0.6367), [10.04397) (95\% CI: 0.2884 - 0.6367), [10.04397) (95\% CI: 0.2884 - 0.6367), [10.04370) (95\% CI: 0.2884 - 0.6370) (95\%$
AUTHOR Menini et al. (34)	ACCURAC	CY METHOD ata Azex and Sheffiel	d test&steriomicros	e-Mail									
Chia et al. (30)	CMM softv	ware PC-DMIS CAD	**	yes									
Marghalini et al. (31) Imburgia et al. (22)	Scanner Ac Optical sca	tivity 880, Smart Op nner (ScanRider, V-C	tic iER srl)	- yes									
Amin et al. (33) Chew et al. (29)	Software G Scanner Ac	eomagic Qualify 12 trivity 880		yes									
Vandeweghe et al. (20) Gimenez-Gonzalez et al. (19) Mangano et al. (21)	Software G CMM Crist 3D: Iscan E	eomagic Qualify 12 ta Apex (Mitutoyo) 01041		yes									
Flugge et al. (13)	Scanner De	ental Laboratorio: D2	50										
Koch et al. (14) Panasnyridakos et al. (32)	Software G Scanner Ev	eomatic traoral: Iscan D103i											
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Gimenez et al. (15) Van der Meer et al. (17)	Scanner Ex CMM Crist Scanner Co	araorat: LAVA Scan ! ta Apex sutact Leitz	51	-									

Table 4: In vitro studies.

Conventional Impressions (CI), Digital Impressions (DI), Intraoral Scanning (IOS), Maxilla (MAX), Mandible (MB), Coordinate measurement machine (CMM), PEEK Scan Bodies (PEEK), Partially edentulous (Part.), Completely edentulous (Compl.), Bone Level (BL), Tissue Level (TL), Splinted (SPT), Not Splinted (NSPT), Open Tray (OT), Closed Tray (CT), Scan Body (SB), Vinyl polysiloxane (VPS), Polyether (PE), Plaster Impression (P).

concluded that the accuracy of impressions with iTero® IOS (Cadent) decreased with the increased length of the scanned section but the angulation of dental implants did not affect scanning accuracy. In 2015, Giménez *et al.* (18) performed a study to assess the accuracy of two different IOS: ZFX Intrascan® (Zimmer Biomet, Dachau Germany) and 3D Progress® (MHT, Verona, Italy), concluding that neither IOS was suitable for taking impressions of dental implants in the full arch. In the same way, Giménez *et al.* (17) concluded that angulated and deep implant placement did not seem to decrease the system's

accuracy with Lava COS® intraoral scanning system (3M ESPE), although accuracy was higher among experienced operators. Also in 2015, the same authors published another *in vitro* study of the CEREC AC Bluecam (Sirona) intraoral scanner. They concluded that neither angulation nor implant depth significantly affected scanner accuracy but operator experience did, with a tendency for less experienced operators to commit lower levels of error (16). In 2017, Giménez-González *et al.* (19) concluded that 3M True Definition IOS (3M ESPE) allows impression taking within the clinically acceptable range *in vitro*, and they identified certain factors that influence accuracy: the amount of visible scanbody, distance and angulation between scan bodies; and operator experience. Vandeweghe *et al.* (20) carried out a study to evaluate the accuracy (trueness and precision) of four IOS in a mandibular model. The authors concluded that the 3M True Definition (3M ESPE) and Trios (3Shape) scanners presented acceptable levels of trueness and precision for dental implant impression taking, but that LAVA COS (3M ESPE) failed to obtain the minimum level of accuracy.

In Vitro -PE-CE

Two *in vitro* studies used digital techniques in (PE) and completely (FE) models (21, 22).

Mangano *et al.* (21) used two models (PEM and FEM) and four IOS. No differences were found in trueness and precision between the IOS; however, differences were found between the PEM and FEM with different IOS. In 2017, Imburgia *et al.* (22) also carried out a study with PEM and FEM, concluding that scanning with IOS was more accurate on the PEM than the FEM, findings that could have important clinical implications.

2. CI vs DI

The twelve articles that compared (CI) with (DI) included four *in vivo* and eight *in vitro* studies.

In Vivo

Comparisons between CI and DI were analyzed in four in vivo studies: a randomized crossover trial (23), two pilot studies (24, 25), and one randomized clinical trial (26). Andriessen et al. (24) assessed the accuracy of IOS (iTero) in edentulous mandibles rehabilitated with overdentures compared with an extraoral laboratory scanner. They concluded that inter-implant distance and implant angulation were critical factors influencing the accuracy of intraoral scanning. Gherlone et al. (25) carried out two cases series studies with a similar design: CE rehabilitated with the "All on Four" protocol. In 2015, CI and DI (LAVA C.O.S scanner, 3M ESPE) were performed, assessing the accuracy of metallic structures through the use of an X-Ray (intraoral digital radiographs). In 2016, the patients were allocated either to the control group (CI) or test group (DI, using the Trios (3Shape). The authors concluded that it is possible to manufacture cobalt-chromium full-arch rehabilitations using computer-aided design/ computer-assisted manufacturing (CAD/CAM) from DI with satisfactory accuracy (26). Joda et al. (23) concluded that in addition to the multiple benefits offered by digital technology, DI allows a more efficient workflow in terms of cost when compared with CI.

In Vitro

The present review included eight *in vitro* studies divided into two subgroups: PE (27-31) and CE (32-34). *In Vitro* - PE

Lee *et al.* (27) compared the models obtained with CI and DI, using a PE customized maxillary model. The

authors reported that there were no statistically significant differences between DI and CI, although statistically significant differences were found with the reference model. Lin *et al.* (28) used four different models with dental implants placed with varying angulation, fabricating definitive casts, observing a decreasing linear trend in deviations for both distance and angle measurements, suggesting that DI was more accurate when the implants diverged more. Marghalini *et al.* (31) found, in their study, which compared CI and DI, that impression techniques could affect accuracy, although within clinically acceptable levels.

Chew *et al.* (29) also evaluated this parameter in two sectional mandibular arch master models with different implants (Straumann Bone Level (BL), and Standard Plus Tissue Level (TL) Straumann, Basel, Switzerland). The authors concluded that for the BL test groups, CI presented significantly lower distortion than DI. In a similar study, Chia *et al.* (30) compared the accuracy of CI versus DI. The authors concluded that CI with 0° angulation between implants was associated with the highest accuracy, although no significant differences were found between different angulations when comparing CI and DI

In Vitro - CE.

In 2016, Papaspyridakos *et al.* (32) did not find significant differences between CI and DI compared with the master cast, with exception of Group II [(Open-Tray non-splinted at implant level) (OPNSPT-BL)]. Menini *et al.* (34) used a CE model with four low-profile implant analogs to evaluate impression accuracy in four different groups: CI (open tray-splinted vs. open tray-no splinted vs. closed tray) and DI (PEEK scanbody, True Definition [3M ESPE]). The authors found that DI achieved higher accuracy than CI. Amin *et al.* (33) used a mandibular model with five inter-foramen analogs in a stone master cast to compare the accuracy of CI and DI, concluding that DI was significantly more accurate than CI.

Discussion

This systematic review was designed to evaluate the accuracy and efficiency of IOS for dental implant impression taking, compared with CI, and to assess the economic feasibility of introducing digital techniques.

The *in vivo* evidence located in the first search was scarce, further reduced by risk of bias determined by the CASP quality assessment (8 studies). So in order to expand the amount of information on the topic, an additional search was carried out expanding the criteria to include *in vitro* studies. In order to critically appraise the works identified, the authors adapted a previously published checklist18 for assessing the potential bias of *in vitro* studies. This checklist was initially designed to evaluate the quality of *in vitro* studies investigating dental materials. However, applying the checklist to the stu-

dies selected in the present review, none fulfilled points 5 to 9. Point 5 of this checklist analyzes sample size, while points 6-9 analyze randomization (sequence generation, allocation concealment mechanism, implementation, and blinding). An in vitro study which evaluates dental implant impression-taking employs a previously designed model, with replicas of dental implants from which impressions are taken. The choice of model does not alter the results, as the models are manufactured industrially in advance and so the rate of error from model to model is negligible. In turn, there is no need for randomization, and sample size does not affect the results obtained. In this way, the authors of the present review used a modified version of the checklist published in 2012 by Faggion et al. (35), removing questions 5-9. In this way, the risk of bias and the quality of the in vitro studies analyzed were assessed by an appropriate, simple, and practical method.

Because of the variability between the *in vivo* studies included and the fact that it was unclear how passive fit had been evaluated, comparisons of the results were not possible (11, 23-26). Likewise, the in vitro studies reviewed could not be compared because of the different methods and IOS employed in both partial (27-31) and completely edentulous model (32-34). Nevertheless, most of the studies analyzed obtained results indicating sufficient accuracy, precision or trueness to guarantee adequate passive fit; especially on partially edentulous models. Several authors concluded that dental implant angulation and depth did not influence outcomes in terms of passive fit (15-17). Regarding the economic feasibility of DI, in comparisons between DI and CI, only a single in vivo study found that DI allowed a more efficient workflow than CI (23).

Nevertheless, four systematic reviews have been conducted evaluating if there are any significant differences in accuracy between CI and DI (one *in vitro* study (36), two *in vivo* (37, 38) studies and one that analyzed both *in vivo* and *in vitro* (39)studies) and all authors have concluded that the quality and quantity of the articles analyzed were insufficient. The present systematic review studied the same issue, analyzing both *in vivo* and *in vitro* studies, and adding one further objective, to determine the economic feasibility of DI.

Conclusions

Based on the data extracted from the articles analyzed in this systematic review, objectives could not be clearly and objectively addressed. It was not possible to determine which implant impression technique leads to better passive fit of superstructures. Digital techniques with intraoral scan impressions offer promising results, although improvements are still needed, particularly in full-arch impression taking. The available *in vivo* evidence is scarce, mainly case reports, which only provided low quality evidence. Randomized clinical studies comparing conventional and digital implant impression techniques are needed to generate decisive evidence. Finally, insufficient evidence was found regarding the economic feasibility of DI for implant-supported restorations, so additional research is needed to clarify this.

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Conflict of Interest

Non declared.